

Individual Differences in Multisensory Processing Are Related to Broad Differences in the Balance of Local versus Distributed Information

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Abstract

The brain's ability to extract information from multiple sensory channels is crucial to perception and effective engagement with the environment, but the individual differences observed in multisensory processing lack mechanistic explanation. We hypothesized that, from the perspective of information theory, individuals with more effective multisensory processing will exhibit a higher degree of shared information among distributed neural populations while engaged in a multisensory task, representing more effective coordination of information among regions. To investigate this, healthy young adults completed an audiovisual simultaneity judgment task to measure their temporal binding window (TBW), which quantifies the ability to distinguish fine discrepancies in timing between auditory and visual stimuli. EEG was then recorded during a second run of the simultaneity judgment task, and partial least squares was used to relate individual differences in the TBW width to source-localized EEG measures of local entropy and mutual information, indexing local and distributed processing

of information, respectively. The narrowness of the TBW, reflecting more effective multisensory processing, was related to a broad pattern of higher mutual information and lower local entropy at multiple timescales. Furthermore, a small group of temporal and frontal cortical regions, including those previously implicated in multisensory integration and response selection, respectively, played a prominent role in this pattern. Overall, these findings suggest that individual differences in multisensory processing are related to widespread individual differences in the balance of distributed versus local information processing among a large subset of brain regions, with more distributed information being associated with more effective multisensory processing. The balance of distributed versus local information processing may therefore be a useful measure for exploring individual differences in multisensory processing, its relationship to higher cognitive traits, and its disruption in neurodevelopmental disorders and clinical conditions.

INTRODUCTION

We experience the world through multiple sensory systems, each sampling different kinds of energy from the environment and offering complementary information about the world around us. The brain's ability to extract relevant information from across sensory channels is critical to interacting effectively with the world, as demonstrated by the numerous behavioral enhancements that multisensory stimuli provide compared with unisensory stimuli (e.g., Shams & Seitz, 2008; Diederich & Colonius, 2004; Hershenson, 1962; Sumby & Pollack, 1954). These enhancements, in combination with converging anatomical and physiological evidence of extensive multisensory influences across neural scales, suggest that the brain is fundamentally organized to facilitate multisensory processing, with wide-reaching consequences for perception, cognition, and action (Driver & Noesselt, 2008; Ghazanfar & Schroeder, 2006).

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Multisensory processing is also characterized by its variability across the population, with substantial individual differences in multisensory tasks and illusions occurring in healthy individuals (e.g., Cecere, Rees, & Romei, 2015; Nath & Beauchamp, 2012; Stevenson, Zemtsov, & Wallace, 2012; Miller & D'Esposito, 2005). Furthermore, correlations among various multisensory tasks and audiovisual illusions suggest that these individual differences may be expressions of a general mechanism of multisensory processing (Stevenson & Wallace, 2013; Stevenson et al., 2012), which may use a set of basic neural operations to flexibly integrate information between distributed neural populations in a wide variety of contexts (van Atteveldt, Murray, Thut, & Schroeder, 2014; Senkowski, Schneider, Foxe, & Engel, 2008). However, prior studies investigating individual differences in multisensory processing have largely focused on univariate measures of neural activity (e.g., Ferri et al., 2017; Balz et al., 2016; Kaganovich & Schumaker, 2016; Cecere et al., 2015) without considering interactions among neural populations (but see Kumar, Dutta, Talwar, Roy, & Banerjee, 2020). Given that multisensory processing involves reconciling information

Journal of Cognitive Neuroscience 34:5, pp. 846–863 https://doi.org/10.1162/jocn_a_01835 encoded in different sensory systems to produce percepts and guide action, we expect that effective multisensory processing requires information to be processed across widely distributed neural populations. As such, we hypothesize that individuals capable of more effective multisensory processing will demonstrate a higher degree of shared information among distributed cortical regions while engaged in a multisensory task, likely including regions of multisensory convergence such as the STS (Jones & Powell, 1970), which is frequently implicated in audiovisual processing (e.g., Marchant, Ruff, & Driver, 2012; Balk et al., 2010; Noesselt et al., 2007; Calvert, Hansen, Iversen, & Brammer, 2001).

To investigate this possibility, we compared the balance of local versus distributed information processing to multisensory performance using information-theoretical measures of local entropy and mutual information at source-localized EEG time series. Multisensory performance was assessed as audiovisual temporal discrimination, employing the commonly used audiovisual simultaneity judgment (SJ) task (e.g., Stevenson & Wallace, 2013; Powers, Hillock, & Wallace, 2009; van Eijk, Kohlrausch, Juola, & van de Par, 2008). This task allows a temporal binding window (TBW) to be measured for each participant, quantifying the probability that an auditory and visual stimulus will be perceived as asynchronous as a function of the time difference between them. TBWs are known to vary substantially between individuals (Stevenson et al., 2012; Powers et al., 2009; Conrey & Pisoni, 2006; Miller & D'Esposito, 2005), and those with narrower TBWs were considered to have more effective multisensory processing, reflecting a better ability to resolve timing differences between sensory channels. Following measurement of the TBW, participants underwent EEG recording during a second run of the SJ task, which was calibrated to equalize difficulty between participants.

To quantify the balance of distributed versus local information processing, source-localized EEG time series were submitted to a time delay embedding-based algorithm computing local entropy and mutual information at multiple timescales (Vakorin, Lippé, & McIntosh, 2011). These information-theoretical measures allow the joint information of two neural time series to be partitioned into that which is unique to each population (local entropy) and that which is shared between them (mutual information). As such, local entropy and mutual information provide measures of local and distributed information, respectively. Partial least squares (PLS; McIntosh & Lobaugh, 2004) was then used to identify components (latent variables [LVs]) of local entropy and mutual information distribution that maximally covaried with the individual-level TBW measurements. Additionally, source-localized power spectral densities (PSDs) were subjected to the same PLS analysis to allow comparison with previous electrophysiological work and disambiguate the role of cross-frequency dependencies and nonlinear autocorrelations in differentiating individuals (Courtiol et al., 2016).

METHODS

Participants

Twenty-eight healthy young adults were recruited, with three being excluded from analysis because of failed sigmoid model fitting after the calibration task (see below) and three excluded for excessive EEG artifacts. The final sample of 22 young adults (11 women, ages 19-33 years, mean = 23.6 years, SD = 3.5 years) had an average of 16.2 years of education, and all had normal or correctedto-normal vision and hearing. Twenty participants were right-handed, one was left-handed, and one was ambidextrous. No participant reported a diagnosis of dyslexia, autism spectrum disorder, schizophrenia, or other clinical condition with noted relevance to multisensory processing (Hahn, Foxe, & Molholm, 2014; de Boer-Schellekens, Eussen, & Vroomen, 2013; Martin, Giersch, Huron, & van Wassenhove, 2013; Kwakye, Foss-Feig, Cascio, Stone, & Wallace, 2011; Foucher, Lacambre, Pham, Giersch, & Elliott, 2007; Hairston, Burdette, Flowers, Wood, & Wallace, 2005). All participants provided written consent according to the guidelines established by Baycrest Centre and the University of Toronto and were provided monetary compensation for their participation.

This work is a secondary analysis of a data set (collected by the authors and previously unpublished) intended to investigate the neural correlates of audiovisual perceptual binding. The final sample size (22) offered by this data set surpassed that of similar work using EEG to investigate multisensory perception during the SJ task (Yuan, Li, Liu, Yuan, & Huang, 2016 [18]; Kambe, Kakimoto, & Araki, 2015 [14]) and is comparable to other EEG studies investigating individual differences in multisensory perception (e.g., Kumar et al., 2020 [18]; Cecere et al., 2015 [22]).

Behavioral Protocol

Audiovisual SJ Task

Participants first completed a two-alternative forcedchoice SJ task to measure the width of their TBWs, as well as to calibrate the stimuli for the task presented during EEG recording. The SJ task consisted of a jittered fixation period (1000–1500 msec), followed by a visual flash and auditory beep stimulus, and lastly a response prompt (see Figure 1). The flash and beep stimuli were separated by a systematically varied SOA, where a negative number denotes auditory-leading (AV) presentation and a positive number denotes visual-leading (VA) presentation.

The auditory stimulus was a 3500-Hz pure sine tone, 10 msec in length, delivered by a GSI 61 audiometer through ER-3A insert earphones (Etymotic Research). The audiometer was calibrated such that a 5-sec tone at the same frequency produced an intensity of 102 dB SPL. The visual stimulus was a white annulus flash on a black background, presented for 10 msec and covering 3.8° of visual angle at a viewing distance of 60 cm. It was presented on a Dell Trinitron CRT monitor at a refresh rate of 100 Hz.



Figure 1. Audiovisual task. Schematic of the audiovisual SJ task depicting the visual-leading (VA) condition.

After an interval of 750 msec, a prompt was displayed, and the participant reported whether they perceived the two stimuli as synchronous ("yes") or asynchronous ("no") by pressing the left or right arrow button (counterbalanced between participants) on a standard computer keyboard. Participants responded with the right hand, and responses were made within a 2000-msec time limit. Trials were then separated by a 750-msec intertrial interval before the next fixation.

The task was built with PsychoPy software (Version 1.90.3; Peirce et al., 2019) and presented on a Dell Precision T3600 computer. Stimulus timing was verified to be accurate within ± 4 msec using a Tektronix TDS210 twochannel oscilloscope.

For the initial calibration run, 19 SOAs were used in total, ranging from -300 to 300 msec, to estimate each participant's TBW. Specifically, SOAs of 0, 10, 20, 50, 80, 100, 150, 200, 250, and 300 msec were presented in both the AV and VA cases (Stevenson et al., 2012). The task was broken into four blocks, wherein each SOA was presented four times in a pseudorandom order, for a total of 16 presentations per SOA. Two hundred eighty-five trials were presented over the course of the whole task, which lasted roughly 15 min in total. Participants were offered a self-timed break between each block.

EEG was recorded during a second run of the SJ task. This version of the task, originally designed to investigate the neural correlates of audiovisual binding, presented six SOAs, four of which were calibrated for each participant individually based on the results of the preceding behavioral run. To do so, the rate of synchrony perception for each SOA was calculated as the number of "synchronous" responses divided by the total number of presentations (16). Two psychometric sigmoid functions—one for the AV SOAs (-300 to 0 msec) and one for the VA SOAs (0–300 msec)—were fit to the resulting rates using the lmfit function in Python (least squares mode; Stevenson & Wallace, 2013; Hillock-Dunn & Wallace, 2012; Powers

et al., 2009). For the AV stimuli, "A50" and "A95" SOAs were calibrated to produce asynchrony perception 50% and 95% of the time, respectively, by solving the AV psychometric sigmoid for values of 0.5 and 0.95. "V50" and "V95" trials were calibrated in the same way for VA stimuli. Lastly, "A10" and "V10" trials used a fixed SOA of 10 msec with auditory- and visual-leading stimuli, respectively. A total of 512 trials were presented in a pseudorandom order, broken into four blocks of 128 trials each. Within each block, A50 and V50 trials were presented 32 times each, and A10, V10, A95, and V95 trials were presented 16 times each. This balance of trial types was chosen to equalize subjective difficulty by presenting participants with a high proportion of ambiguous stimuli while preventing guessing or adaptation by offsetting these with more obviously synchronous (A10, V10) and asynchronous (A95, V95) stimuli.

Observer Model

Although an arbitrary psychometric sigmoid was used to calibrate the ambiguous stimuli at the time of data collection, a more sophisticated observer model was applied post hoc to parameterize the TBW. The four parameter observer model proposed by Yarrow et al. (Yarrow, 2018, 2020; Yarrow, Jahn, Durant, & Arnold, 2011) posits that SIs are the product of a latent decision process, where a noisy internal representation of the difference in timing between stimuli is compared with lower (auditoryleading) and upper (visual-leading) decision criteria. The TBW is therefore estimated as the difference of two cumulative Gaussians representing the noisy boundaries separating simultaneous from nonsimultaneous judgments. Each Gaussian is defined by a mean (m_{AV} and $m_{\rm VA}$; the estimated mean SOA values of the decision criteria) and standard deviation (σ_{AV} and σ_{VA} ; representing a combination of sensory and criterion noise). As such, $m_{\rm AV}$ and $m_{\rm VA}$ define the width of the TBW and are analogous to other point estimates of TBW width, which have previously shown individual differences (e.g.. Stevenson et al., 2012; Powers et al., 2009; Conrey & Pisoni, 2006; Miller & D'Esposito, 2005), whereas σ_{AV} and σ_{VA} determine the slope of the TBW. In line with previous work, m_{AV} and m_{VA} were considered the primary measures of interest quantifying individual differences in the multisensory SJ task and will hereafter be referred to simply as the AV and VA TBW width, respectively.

To assess the fit of the observer model, it was compared with a simpler two-parameter "guessing" model, designed to determine whether participants were simply guessing and whether they were presented with a sufficient range of SOAs to adequately sample their transitions from simultaneous to nonsimultaneous judgments. Full details of the observer model, the guessing model, and their implementation are available in Yarrow et al. (Yarrow, 2018, 2020; Yarrow et al., 2011).

Self-report Measures

Participants completed a posttask questionnaire, the results of which were not analyzed here. Participants reflected on the SJ task and tried to quantify potential biases in their responding, as well as guess the intention of the study. Additional questions assessed discomfort and whether participants fell asleep at any point during the task, as well as clinical or neurodevelopmental diagnoses (e.g., dyslexia, autism spectrum disorder, and schizophrenia). Finally, participants reported their experience with and time spent playing video games, as well as musical training and proficiency.

Electrophysiological Analysis

EEG Recording and Preprocessing

EEG was recorded with a BioSemi ActiveTwo acquisition system (BioSemi Instrumentation) at a sampling rate of 2048 Hz and bandwidth (-3 dB) of DC-400 Hz and then decimated to 512 Hz in ActiView acquisition software. Sixty-six scalp electrodes were employed, using BioSemi's 64 + 2 electrode cap configuration based on the 10/20 system. Ten additional electrodes were applied in pairs to the mastoids, preauricular points, upper cheeks, outer canthi of the eyes, and inferior orbit of the eyes. These provided better coverage of the scalp, as well as an accurate record of eye movements for later artifact removal. All recordings took place in a dimly lit, sound-attenuating room.

All EEG preprocessing was performed in Brainstorm (Version 07-Apr-2020; Tadel, Baillet, Mosher, Pantazis, & Leahy, 2011), an open-source application for M/EEG data processing and visualization. Continuous recordings were digitally band-pass filtered at 0.5–90 Hz (linear-phase FIR, stopband attenuation = 60 dB, transition band = 0 Hz), with a notch filter centered at 60 Hz to attenuate line noise (second-order IIR, 3-dB notch bandwidth = 2 Hz). Bad

electrodes and contaminated segments of continuous data were manually rejected from subsequent processing, and the remaining data were rereferenced to the average of all remaining electrodes. Eye- and cardiac-related artifact components were then detected and removed using Brainstorm's implementation of Infomax independent component analysis (Makeig, Bell, Jung, & Sejnowski, 1996) applied to the longest available continuous segment of data without major artifacts (minimum of 5 min or 153,600 samples).

We assessed individual differences in neural activity during the multisensory task by analyzing data from the intertrial interval, with epochs spanning 1750 msec starting immediately after the response and ending before the onset of the next stimulus. This interval was chosen to capture individual differences in the functional organization of brain activity that emerges during the multisensory task while minimizing spillover from the stimuli themselves, which varied between participants and could not be directly compared. Implications of this choice are addressed in the Discussion section. After rejection of contaminated segments, an average of 471.4 epochs of 1750 msec (13.7 min of data in total) were analyzed for each participant.

EEG Source Estimation

The cortical current sources of the EEG signals were estimated with Brainstorm using sLORETA (Pascual-Marqui, 2002), with one dipole modeled normal to the cortical surface at each vertex, using an OpenMEEG BEM forward model (Gramfort, Papadopoulo, Olivi, & Clerc, 2010) computed on the default MNI/ICBM152 anatomy in Brainstorm (Fonov, Evans, Mckinstry, Almli, & Collins, 2009). The inversion kernel computed on the full cortical surface (15,002 vertices) was used to downsample the results to the Desikan-Killiany atlas (Desikan et al., 2006), resulting in one time series for each of the 68 regions of the atlas.

PSD Computation

PSDs were computed using a smoothed fast Fourier transform implemented in the *neurodsp* package in Python ("medfilt" method, frequency range = 1-90 Hz, frequency resolution = 0.57 Hz, median filter length = 1 Hz; Cole, Donoghue, Gao, & Voytek, 2019). PSDs were computed on each individual epoch and then averaged over epochs, resulting in one average PSD associated with each source.

Local Entropy and Mutual Information

Entropy H(X) is a measure of information or uncertainty associated with a single random variable *X*. Similarly, the joint entropy H(X, Y) is the entropy of the joint probability distribution of two random variables *X* and *Y*. By conceptualizing neural time series as random variables, information theory provides tools to partition the joint entropy of



Figure 2. Mutual information and local entropy. The total entropy H(X, Y) of two neural time series (*X* and *Y*) can be partitioned into shared and unique quantities. Mutual information, I(X; Y), is the shared entropy between *X* and *Y* and is therefore a measure of affiliation between the two variables. H(X|Y) and H(Y|X) are estimates of the local (unique) entropy of each variable, representing the remaining entropy after knowledge of the other variable (mutual information) is excluded.

two neural time series into that which is unique to one or the other (local entropy) and that which is shared between them (mutual information; see Figure 2).

Partitioning of the joint entropy of *X* and *Y* can be described with the following formula:

$$H(X,Y) = H(X|Y) + H(Y|X) + I(X;Y)$$

The conditional entropies H(X|Y) and H(Y|X), referred to here as local entropies, represent the entropy of each time series with knowledge of the other excluded. The mutual information I(X; Y) between X and Y therefore represents the amount of information shared between the two variables.

Local entropy and mutual information were estimated with time delay embedding (embedding dimension d =2, embedding delay $\tau = 1$, characteristic scale length r =1) using the method previously described in Vakorin et al. (2011). Given that entropy estimates are scale dependent (Costa, Goldberger, & Peng, 2005; Zhang, 1991), these quantities were computed at multiple timescales. To do so, each time series was downsampled by averaging within nonoverlapping windows of successively increasing length before time delay embedding. A maximum window length of 18 samples was chosen to ensure that a minimum of about 50 data points (896 samples/18 = 49.78 windows) were included in the estimation.

To characterize the dynamic interactions of the wholebrain network, multiscale local entropy and mutual information were computed between each pair of sources at each epoch and then averaged across epochs. Local entropy for a given node X was then taken to be the average of local entropy values, H(X|Y), computed between that node and all other nodes Y.

PLS Analysis

PLS (McIntosh & Lobaugh, 2004; McIntosh, Bookstein, Haxby, & Grady, 1996) is a multivariate statistical technique, similar to canonical correlation, which uses singular value

decomposition (SVD) to extract orthogonal patterns of maximal covariance, called LVs, between two data matrices. PLS can therefore identify components of a brain data matrix that maximally covary with behavioral measurements. Specifically, the relationship between brain and behavior data, represented by their cross-product matrix, is decomposed using SVD, producing three new matrices, containing (1) behavior saliences, (2) brain saliences, and (3) singular values. The behavior saliences can be thought of as contrasts that specify the relationship between the elements of the behavioral matrix, and the "brain saliences" are the extracted patterns of brain data that best characterize the cross-product matrix. The singular values are the square roots of the eigenvalues and are proportional to the amount of covariance in the cross-product matrix captured by each LV. Finally, because the extraction of these brain-behavior relationships via SVD takes place across the entire brain in a single mathematical step, correction for multiple comparisons is not necessary (McIntosh & Lobaugh, 2004; McIntosh et al., 1996).



Figure 3. TBW estimates. (A) Average TBW for the whole sample. By convention, negative SOAs denote auditory-leading (AV) stimuli and positive SOAs denote visual-leading (VA) stimuli. Shading depicts *SEM*. (B) Relationship between AV and VA TBW width estimates. TBW widths (AV and VA) were quantified for each participant as the means of the two cumulative Gaussians from that participant's observer model fit (Yarrow, 2018, 2020).

Here, behavior PLS implemented in MATLAB (McIntosh & Lobaugh, 2004) was used to identify LVs relating individual differences in TBW width to patterns in (1) local entropy, (2) mutual information, and (3) PSDs. To explore the maximal experimental effects in the data, the rotated version of PLS was used, which produces a set of LVs based on mutually orthogonal contrasts in a data-driven manner. Statistical assessment of the resulting LVs was performed with a two-stage resampling procedure. First, statistical significance of each LV was estimated using permutation testing (1000 resamples), where observations of the behavioral matrix were randomly reassigned without replacement. The resulting p value represents the proportion of permuted singular values that exceeded the observed singular values. The reliability of each element was then estimated using bootstrap resampling (1000 resamples), where the standard error of each element salience was estimated by recomputing PLS on a set of observations resampled with replacement (maintaining the mapping between brain and behavioral observations). The bootstrap ratio (the ratio of the salience to the standard error computed through resampling) captures how dependent the element salience is on the particular makeup of the sample (Sampson, Streissguth, Barr, & Bookstein, 1989), and is roughly equivalent to a z score when the bootstrap



Figure 4. Local entropy PLS results. (A) Data-driven contrast for PLS relating AV and VA TBW width to local entropy, with *p* values derived from 1000 permutations. (B) LV1 bootstrap ratios at each source and timescale. Bootstrap ratios quantify the stability of the contrast at each source and timescale as determined through bootstrap resampling. Negative values here indicate sources and timescales where narrower TBWs are associated with less local entropy. (C) Distribution of LV1 bootstrap ratios across all sources. (D) LV1 bootstrap ratios at each source as a function of timescale.

distribution is normal (Efron & Tibshirani, 1986). We therefore interpret the bootstrap ratios as measures of reliability, using the permutation test for null hypothesis testing.

RESULTS

Observer Model Fitting

The observer model provided a significant improvement in fit over the guessing model in all cases (p < .001; Appendix A), suggesting that participants were not guessing, and SOAs were adequately sampled.

The mean TBW width estimated with the observer model was 162.1 msec (SD = 59.3 msec) for AV stimuli and 236.0 msec (SD = 86.44 msec) for VA stimuli, reproducing the commonly reported finding that the TBW is wider for VA stimuli than AV stimuli on average, t(21) = -5.9, p < .001.¹ Figure 3A depicts the average TBW for all participants in the sample. As described previously (e.g., Stevenson et al., 2012), AV and VA TBW widths were strongly correlated within individuals, r(20) = .75, p < .001 (see Figure 3B).

Local Entropy

Behavior PLS relating local entropy values to TBW width identified one significant LV (LV1: p < .001, singular value = 18.58; LV2: p = .70, singular value = 3.28). Figure 4 illustrates the relationship between TBW width and local entropy estimates across sources and timescales captured by this LV. The data-driven contrast values for AV and VA TBW width had the same sign (see Figure 4A, left), indicating that this LV captures commonalities between the two measures in their relation to local entropy. For this LV, correlations [95% CI] between brain scores and TBW width were AV: -.75 [-.89, -.67] and VA: -.67 [-.85, -.55]. Bootstrap ratios quantify the stability of this contrast at each source and timescale, where positive ratios indicate support for the contrast and negative ratios indicate support for the inverse of the contrast. Because the contrast values in this case are negative, negative bootstrap ratios indicate where TBW width and local entropy are positively related. Bootstrap ratios were overwhelmingly negative across sources and timescales (see Figure 4B–D), indicating that narrower TBWs were associated broadly with lower local entropy, and therefore, wider TBWs were associated with higher local entropy. Furthermore, the effect was most stable at finer timescales, with the 11.7 msec timescale having the most extreme median bootstrap ratio. Table 1A lists the sources demonstrating the highest median bootstrap ratios across timescales.

In addition to the width parameters, the slope parameters were also compared with local entropy values using behavior PLS. Whether relating local entropy to width and slope together (Appendix Figure B1, left side) or slope **Table 1.** The 10 Sources with the Most Extreme Median PLSBootstrap Ratios for (A) Local Entropy and (B) MutualInformation, Computed Across All Timescales

Source	Median Bootstrap Ratio
(A) Local Entropy	
Pars triangularis R	-4.98
Caudal anterior cingulate R	-4.75
Middle temporal R	-4.49
Superior temporal R	-4.38
Caudal anterior cingulate L	-4.28
Superior frontal L	-4.22
Pars opercularis R	-3.80
Caudal middle frontal R	-3.72
Superior frontal R	-3.59
Fusiform R	-3.56
(B) Mutual Information	
Middle temporal R	2.60
Rostral middle frontal R	2.46
Pars triangularis R	2.44
Pars orbitalis R	2.14
Caudal anterior cingulate R	2.13
Paracentral R	2.12
Superior temporal R	2.10
Superior frontal L	2.05
Rostral middle frontal L	2.03
Pars triangularis L	1.97

Sources in **bold** are within the top 10 for both local entropy and mutual information. R = right; L = left.

alone (Appendix Figure B1, right side), the pattern that emerged was largely the same as that described above.

Mutual Information

PLS relating mutual information to TBW width identified one significant LV (LV1: p = .005, singular value = 125.96; LV2: p = .70, singular value = 27.88). Figure 5 depicts the expression of this LV across timescales and source-to-source connections. The data-driven contrast values for AV and VA TBW width again had the same sign (see Figure 5A, left), indicating that this LV captures commonalities between the two measures in their relationship to mutual information. For this LV, correlations [95% CI] between brain scores and TBW width were AV: -.63 [-.85, -.54] and VA: -.71 [-.88, -.65]. In contrast to local entropy, the bootstrap ratios for mutual



Figure 5. Mutual information PLS results. (A) Data-driven contrast for PLS relating AV and VA TBW width to mutual information, with p values derived from 1000 permutations. (B) Number of times the given source was involved in a highly reliable (bootstrap ratio > 4) connection with any other source. Bootstrap ratios here quantify the stability of the contrast at each source-to-source connection and timescale as determined through bootstrap resampling. Positive values here indicate connections where narrower TBWs are associated with higher mutual information. (C) Distribution of LV1 bootstrap ratios across all source-to-source connections. (D) Number of source-to-source connections with LV1 bootstrap ratios exceeding 4 as a function of timescale.

information were predominantly positive, indicating that narrower TBWs were largely associated with higher mutual information across timescales and connections, and therefore, wider TBWs were associated with lower mutual information. Again, this effect was most stable at finer timescales. Table 1B lists the sources with the highest median bootstrap ratios across timescales, which are most prominently involved in this pattern, and Figure 5B depicts the number of times a given source is involved in a highly reliable (bootstrap ratio > 4) connection with any other source. To illustrate the pattern of connectivity itself, Figure 6 displays the pattern of connections exhibiting the highest reliability at the 11.7-msec timescale. The slope parameters were also compared with mutual information using behavior PLS. Relating mutual information to width and slope together revealed a similar pattern to the one described above (Appendix Figure C1, left side); however, slope alone did not yield any significant LVs (Appendix Figure C1, right side).

PSD

PLS relating PSDs to TBW width extracted two LVs, but permutation testing indicated that neither was significant (LV1: p = .28, singular value = 31.41; LV2: p = .73, singular value = 9.71). **Figure 6.** Mutual information PLS results: connectivity. Circle plot depicting the 1% of connections with the highest bootstrap ratios for the 11.7 msec timescale. Positive values indicate connections where narrower TBWs are associated with higher mutual information. Top left inset: Connections with LV1 bootstrap ratios exceeding 4 as a function of timescale. Red line marks the timescale featured in the circle plot.



DISCUSSION

Narrower TBW Is Broadly Associated with Mutual Information and Negatively Associated with Local Entropy

We found that individual differences in audiovisual temporal discrimination ability, as measured by TBW width covaried with differences in local entropy and mutual information while participants engaged in an audiovisual task. Widespread differences were observed, with better temporal discrimination (narrower TBW) being associated with higher mutual information and lower local entropy broadly across cortical sources and timescales. Taken together, these results support the hypothesis that better multisensory processing abilities are associated with a propensity for greater shared information among distributed cortical sources and, conversely, less effective processing is associated with more localized processing of information. A potential interpretation of this finding is that the ability to extract stimulus features (e.g., timing) encoded in separate modalities, compare them, and respond appropriately is facilitated in individuals who show broad integration of information involving the coordination of diverse neural populations while engaged in a multisensory task.

Furthermore, for both local entropy and mutual information, only the LV capturing similarities between the AV and VA TBW widths passed statistical assessment, suggesting that the pattern of mutual information and local entropy identified in the brain data applies to both types of stimulus. This finding, along with the strong correlation observed between AV and VA TBWs, accords with previous work proposing that the TBW width indexes a general mechanism of multisensory processing that applies across stimulus types (Stevenson et al., 2012), although further work comparing multiple tasks will be necessary to confirm this. Moreover, if local entropy and mutual information balance do reflect domain-general multisensory processing ability, further work will need to consider how this more general process interacts with possible stimulus-specific mechanisms, which may produce the observed difference in neural responses to AV and VA stimuli (e.g., Cecere, Gross, Willis, & Thut, 2017) and differences in the malleability of the AV and VA TBWs (Cecere, Gross, & Thut, 2016; Powers et al., 2009).

Although TBW width was our primary measure of interest, the observer model also provides the slope of the TBW, and these two parameters have different theoretical interpretations. Under the assumptions of the observer model, width indexes the position of the boundary between simultaneous and nonsimultaneous judgments, whereas slope is hypothesized to capture the "noisiness" of internal representations of stimulus timing and decision criteria. Despite these theoretical differences, our results suggest that both width and slope relate to largely the same pattern of individual differences in local entropy and mutual information (Appendices B and C). It could be the case that the observer model is correct in its interpretation of these parameters, but they are too strongly correlated to disambiguate (i.e., noisy observers may tend to also have noisy criteria; Magnotti, Ma, & Beauchamp, 2013). Alternatively, the model may not reflect the underlying process that produced these simultaneity judgments accurately enough to afford such specific interpretation of its parameters. In either case, we can only conclude that the individual differences observed in the brain data correspond to general performance on the SJ task, rather than criterion setting or the noisiness of internal representations specifically.

Temporal and Frontal Regions Exhibit Most Reliable Differences in Local Entropy and Mutual Information

Although narrower TBWs were associated with more distributed and less localized information processing broadly throughout the cortex, the most reliable differences were observed primarily in temporal and frontal cortex (see Table 1). Several of these temporal regions (right superior temporal gyrus and right middle temporal gyrus) and frontal regions (right pars triangularis, right caudal anterior cingulate, and left superior frontal gyrus) were among those that most reliably demonstrated an effect in both the local entropy and mutual information analyses.

Of particular interest is the STS, which has historically been considered a key region for multisensory processing because of its converging auditory and visual inputs (Jones & Powell, 1970), and the nonhuman primate work demonstrating the presence of neurons responsive to both modalities there (Schroeder & Foxe, 2002; Bruce, Desimone, & Gross, 1981; Benevento, Fallon, Davis, & Rezak, 1977). In humans, numerous fMRI studies have implicated STS (Marchant et al., 2012; Balk et al., 2010; Noesselt et al., 2007; Calvert et al., 2001), as well as nearby superior temporal gyrus (Marchant et al., 2012; Stevenson, VanDerKlok, Pisoni, & James, 2011; Stevenson, Altieri, Kim, Pisoni, & James, 2010; Noesselt et al., 2007) in the integration or temporal discrimination of asynchronous auditory and visual stimuli using a variety of task paradigms, which motivated our prediction that STS would be linked to individual differences on this task. Given the limited spatial resolution of the present analysis, it is plausible that the prominent differences observed in the right superior temporal and right middle temporal sources could originate in the STS and superior temporal gyrus. If so, these results would suggest that individual variability in audiovisual temporal discrimination may in part reflect the degree to which these putatively multisensory temporal regions exchange information with a wide array of other cortical regions (see Figure 6). However, it is important to note that these sources are based on atlas parcellations encompassing large areas of cortex, likely including multiple subregions that play diverse roles in cognition (Hein & Knight, 2008). Therefore, the sources used here may capture different processes than those reported in the fMRI literature. Furthermore, in contrast to previous findings, here the most reliable effects in temporal cortex were observed in the right hemisphere, with little

difference emerging in the left hemisphere. Although the fMRI literature shows largely left-hemispheric or bilateral effects at the group level, the emphasis here on individual differences means that this is not necessarily a contradictory finding (but see Marchant et al., 2012). This discrepancy may be the result of heterogeneity in task design as well as inherent differences between the BOLD signal and information-theoretical measures used here. Alternatively, this finding could indicate that left multisensory temporal cortex is more consistently implicated in audiovisual processing tasks, but the degree to which right multisensory temporal cortex is involved varies between individuals and may be more closely related to performance. This individual variability in the involvement of right multisensory temporal cortex could therefore explain why it is less consistently identified using BOLD signal contrasts computed at the group level. Future work seeking to clarify the networks involved in multisensory processing may therefore benefit from considering how individual differences in these networks may relate to task performance.

In frontal cortex, a particularly strong relationship was identified between bilateral caudal anterior cingulate and TBW width. In particular, higher local entropy in this region was strongly associated with wider TBWs, especially at finer timescales. Involvement of this region in a forcedchoice task is not unexpected, given that ACC has been implicated in decision-making and action selection in general and is thought to play a flexible role in integrating behaviorally relevant information from its prefrontal, parietal, and subcortical connections (Monosov, Haber, Leuthardt, & Jezzini, 2020). Furthermore, there is evidence that ACC is capable of integrating information over long timescales, including those spanning multiple trials (Spitmaan, Seo, Lee, & Soltani, 2020). Although still speculative, this result could suggest that individual differences in TBW may, to some extent, reflect differences in response selection processes mediated by ACC and its network, perhaps involving the way information from previous trials is integrated to affect response selection.

Differences in Local Entropy and Mutual Information Most Evident at Fine Timescales

In addition to spatial information, the current method gives insight into the temporal scales where individual differences in the information-theoretical measures most reliably correspond to individual differences in TBW. Although some sources exhibited differences across all timescales, the finer timescales were most consistently identified for both local entropy and mutual information, with median bootstrap ratios peaking at the 11.7 msec timescale for local entropy and decreasing monotonically from fine to coarse timescales for mutual information. Because the downsampling procedure removes the influence of fastchanging activity as the coarse-graining windows become larger, fine timescales represent the entropy of both fastand slow-changing activity, whereas coarser timescales represent only slow-changing activity (Courtiol et al., 2016). This suggests that the key individual differences in local entropy and mutual information are likely attributable to relatively fast-changing elements of the neural signals. This finding would seem to corroborate the view that gamma synchronization between distinct neuronal groups may play an instrumental role in structuring information within cortical networks in general (Fries, 2009; Engel, Fries, & Singer, 2001) as well as the orchestration of multisensory interactions more specifically (Keil & Senkowski, 2018). However, relating power spectra to the width of the TBW with PLS did not show differences in power in the gamma range or any other, highlighting the fact that straightforward comparisons between the (multiscale) entropy measure used here and the power spectrum are likely not possible. Simulation work has demonstrated that multiscale entropy (Costa et al., 2005), a similar technique to that used here, is sensitive to nonlinear autocorrelations in the time series, as well as crossfrequency dependencies, although this is not true of the power spectrum (Courtiol et al., 2016; McIntosh, Kovacevic, & Itier, 2008). These differences confirm that the information-theoretical measures provide additional insight into the temporal structure of neural signals at fine timescales, which is not captured in the power spectrum.

Implications of Task Design

Given the substantial variability in performance on the SJ task, the SOAs were calibrated to equalize difficulty across participants (Yuan et al., 2016; Kambe et al., 2015). For the present analysis, the choice to vary stimuli between participants comes with a trade-off, namely, that stimulus-related activity cannot be compared directly between individuals. Although this is not ideal, the particularities of the neural responses to each type of stimulus (i.e., AV and VA) is of secondary interest to individual differences in the broader context of information processing that emerged during the task, which we judged more likely to relate to general (i.e., nonstimulus specific) mechanisms of multisensory processing. Furthermore, focusing on the intertrial interval allowed longer epochs without motor contamination to be analyzed and therefore allowed longer timescales to be assessed. Lastly, equalizing task difficulty across participants is intended to prevent the boredom or blind guessing that comes with a task that is too easy or too difficult, respectively, which are problematic when participants are assumed to be comparably engaged in the task.

The use of the intertrial interval in this analysis, rather than task-free resting-state data, poses additional questions for interpretation. Task-free resting-state data are typically assumed to better reflect inherent differences in functional organization between individuals, as opposed to the more transient brain states related to a specific task. However, the assumption that task-free resting-state provides an inherently neutral baseline reading of brain organization or that such a baseline can exist has been questioned on both procedural and theoretical grounds (Duncan & Northoff, 2013; Morcom & Fletcher, 2007), and evidence from fMRI work suggests that engaging participants in a task may in fact enhance behaviorally relevant individual differences compared with rest (Finn et al., 2017). With this in mind, we judged the intertrial interval sufficient to identify the task-related individual differences of interest; however, future work may need to consider both recordings made during multisensory tasks as well as task-free rest to disambiguate this issue.

Conclusion and Future Directions

Partitioning entropy into local and distributed components provided new insight into the neural correlates of individual differences in multisensory processing commonly observed in healthy adults and served as a proof of principle for the utility of information-theoretical measures for investigating multisensory processing. Overall, more effective multisensory processing, here operationalized as a narrower audiovisual TBW, was associated with a widespread pattern of higher mutual information and lower local entropy while participants were engaged in an audiovisual SJ task. This pattern provides support for the hypothesis that more effective multisensory processing requires sharing of information between widely distributed neural populations. Furthermore, several regions were strongly implicated in this pattern, including temporal and frontal regions that have previously been linked to multisensory integration and response selection, respectively. This suggests that the involvement of these regions within the larger pattern of information exchange could be important determinants of individual differences in multisensory processing.

To more definitively establish the causal role that the distribution versus localization of information plays in individual multisensory performance, future work will need to adopt an experimental approach. Prior work has shown that the TBW can be narrowed with training (Stevenson, Wilson, Powers, & Wallace, 2013; Powers et al., 2009) and that such training produces changes in resting-state and task-related BOLD functional connectivity among a network of unisensory and multisensory areas, including the posterior STS (Powers, Hevey, & Wallace, 2012). Training could be combined with the information-theoretical approach used here to test whether pre- and posttraining comparisons identify similar differences in local and distributed information processing throughout the brain. Furthermore, comparing local entropy and mutual information across multiple multisensory tasks could distinguish effects related to the particularities of each task from those related to a more general mechanism of multisensory processing and/or response selection underlying the correlation between tasks (van Atteveldt et al., 2014; Stevenson & Wallace, 2013; Stevenson et al., 2012).

Lastly, given the widespread nature of the individual differences in local entropy and mutual information, this perspective may help explain the links between individual differences in multisensory processing and higher-order cognitive abilities (see Wallace, Woynaroski, & Stevenson, 2020, for a review), such as those between multisensory RT benefit and intelligence in children (Barutchu et al., 2011), TBW width and problem solving in young adults (Zmigrod & Zmigrod, 2016), and

audiovisual detection and mild cognitive impairment in older adults (Murray et al., 2018). Similarly, this approach may also shed light on mechanisms of dysfunction in clinical and neurodevelopmental groups with abnormalities in multisensory processing such as schizophrenia (Martin et al., 2013; Foucher et al., 2007), autism spectrum disorder (de Boer-Schellekens et al., 2013; Kwakye et al., 2011), and dyslexia (Hahn et al., 2014; Hairston et al., 2005).

APPENDIX A

Figure A1. Observer model versus guessing model likelihood ratios. The observer model fit was compared with a two-parameter guessing model for each participant (Yarrow, 2018, 2020). The likelihood ratio was calculated as likelihood ratio = $-2 \log$ likelihood_{guess model} - (-2 log likelihood_{observer model}), and the resulting ratio was compared with the chi-square distribution (df = 2). The observer model provided a superior fit for all participants (all likelihood ratios >13.82, p < .001, indicating that participants were likely not guessing, and the range of SOAs used adequately sampled both transitions (AV and VA) from simultaneous to nonsimultaneous perception.



APPENDIX B



Figure B1. Local entropy and observer model parameters—extended PLS results. Left side: Behavior PLS relating all four observer model parameters (AV and VA width and slope) to local entropy. Only the first LV was significant (LV1: p < .001, singular value = 22.11; LV2: p = .79, singular value = 5.89, LV3: p = .92, singular value = 4.48, LV4: p = .71, singular value = 3.23). Note that AV slope and VA slope represent the observer model parameters σ_{AV} and σ_{VA} , respectively, therefore lower values represent steeper slopes and a sharper transition between simultaneous and nonsimultaneous judgments. (A) Data-driven contrast for PLS relating all four observer model parameters to local entropy (first LV only), with p values derived from 1000 permutations. (B) LV1 bootstrap ratios relating all four observer model parameters to local entropy at each source as a function of timescale. Right side: Behavior PLS relating just the AV and VA slope observer model parameters to local entropy. Only the first LV was significant (LV1: p = .037, singular value = 13.05; LV2: p = .50, singular value = 5.26). (C) Data-driven contrast for PLS relating the observer model slope parameters to local entropy (first LV only), with p values derived from 1000 permutations. (D) LV1 bootstrap ratios relating the observer model slope parameters to local entropy at each source as a function of timescale.



Figure C1. Mutual information and observer model parameters—extended PLS results. Left side: Behavior PLS relating all four observer model parameters (AV and VA width and slope) to mutual information. Only the first LV was significant (LV1: p = .001, singular value = 146.91; LV2: p = .97, singular value = 47.73; LV3: p = .91, singular value = 34.56; LV4: p = .72, singular value = 27.61). Note that AV slope and VA slope represent the observer model parameters σ_{AV} and σ_{VA} , respectively; therefore, lower values represent steeper slopes and a sharper transition between simultaneous and nonsimultaneous judgments. (A) Data-driven contrast for PLS relating all four observer model parameters to mutual information (first LV only), with p values derived from 1000 permutations. (B) Number of times the given source was involved in a highly reliable (bootstrap ratio > 4) connection with any other source. Right side: Behavior PLS relating just the AV and VA slope observer model parameters to mutual information (first LV only), with p values derived from 1000 permutations (LV1: p = .16, singular value = 88.48; LV2: p = .81, singular value = 36.69). (C) Data-driven contrast for PLS relating the observer model slope parameters to mutual information (first LV only), with p values derived from 1000 permutations. (D) Number of times the given source was involved in a highly reliable (bootstrap ratio > 4) connection with any other source.

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Diversity in Citation Practices

Retrospective analysis of the citations in every article published in this journal from 2010 to 2021 reveals a persistent pattern of gender imbalance: Although the proportions of authorship teams (categorized by estimated gender identification of first author/last author) publishing in the Jour*nal of Cognitive Neuroscience (JoCN)* during this period were M(an)/M = .407, W(oman)/M = .32, M/W = .115, and W/W = .159, the comparable proportions for the articles that these authorship teams cited were M/M = .549, W/M = .257, M/W = .109, and W/W = .085 (Postle and Fulvio, JoCN, 34:1, pp. 1-3). Consequently, JoCN encourages all authors to consider gender balance explicitly when selecting which articles to cite and gives them the opportunity to report their article's gender citation balance. The authors of this article report its proportions of citations by gender category to be as follows: M/M = .574, W/M = .296, M/W = .093, and W/W = .037.

Note

1. Nearly identical results were obtained from the arbitrary sigmoid fit at the time of data collection, with the width of the sigmoid at 50% simultaneity perception correlating almost perfectly with the width estimated from the observer model (Pearson's r = .99 for AV stimuli and r = .98 for VA stimuli).

REFERENCES

- Balk, M. H., Ojanen, V., Pekkola, J., Autti, T., Sams, M., & Jääskeläinen, I. P. (2010). Synchrony of audio-visual speech stimuli modulates left superior temporal sulcus. *NeuroReport*, 21, 822–826. https://doi.org/10.1097/WNR.0b013e32833d138f, PubMed: 20588202
- Balz, J., Keil, J., Roa Romero, Y., Mekle, R., Schubert, F., Aydin, S., et al. (2016). GABA concentration in superior temporal sulcus predicts gamma power and perception in the sound-induced flash illusion. *Neuroimage*, *125*, 724–730. https://doi.org/10.1016/j.neuroimage.2015.10.087, PubMed: 26546865
- Barutchu, A., Crewther, S. G., Fifer, J., Shivdasani, M. N., Innes-Brown, H., Toohey, S., et al. (2011). The relationship between multisensory integration and IQ in children. *Developmental Psychology*, 47, 877–885. https://doi.org/10 .1037/a0021903, PubMed: 21142364

- Benevento, L. A., Fallon, J., Davis, B. J., & Rezak, M. (1977). Auditory–visual interaction in single cells in the cortex of the superior temporal sulcus and the orbital frontal cortex of the macaque monkey. *Experimental Neurology*, *57*, 849–872. https://doi.org/10.1016/0014-4886(77)90112-1, PubMed: 411682
- Bruce, C., Desimone, R., & Gross, C. G. (1981). Visual properties of neurons in a polysensory area in superior temporal sulcus of the macaque. *Journal of Neurophysiology*, 46, 369–384. https://doi.org/10.1152/jn.1981.46.2.369, PubMed: 6267219
- Calvert, G. A., Hansen, P. C., Iversen, S. D., & Brammer, M. J. (2001). Detection of audio-visual integration sites in humans by application of electrophysiological criteria to the BOLD effect. *Neuroimage*, 14, 427–438. https://doi.org/10.1006 /nimg.2001.0812, PubMed: 11467916
- Cecere, R., Gross, J., & Thut, G. (2016). Behavioural evidence for separate mechanisms of audiovisual temporal binding as a function of leading sensory modality. *European Journal of Neuroscience*, 43, 1561–1568. https://doi.org/10.1111/ejn .13242, PubMed: 27003546
- Cecere, R., Gross, J., Willis, A., & Thut, G. (2017). Being first matters: Topographical representational similarity analysis of ERP signals reveals separate networks for audiovisual temporal binding depending on the leading sense. *Journal* of Neuroscience, 37, 5274–5287. https://doi.org/10.1523 /JNEUROSCI.2926-16.2017, PubMed: 28450537
- Cecere, R., Rees, G., & Romei, V. (2015). Individual differences in alpha frequency drive crossmodal illusory perception. *Current Biology*, 25, 231–235. https://doi.org/10.1016/j.cub .2014.11.034, PubMed: 25544613
- Cole, S., Donoghue, T., Gao, R., & Voytek, B. (2019). NeuroDSP: A package for neural digital signal processing. *Journal of Open Source Software*, 4, 1272. https://doi.org/10.21105 /joss.01272
- Conrey, B., & Pisoni, D. B. (2006). Auditory–visual speech perception and synchrony detection for speech and nonspeech signals. *Journal of the Acoustical Society of America*, 119, 4065–4073. https://doi.org/10.1121/1.2195091, PubMed: 16838548
- Costa, M., Goldberger, A. L., & Peng, C. K. (2005). Multiscale entropy analysis of biological signals. *Physical Review E*, 71, 1–18. https://doi.org/10.1103/PhysRevE.71.021906, PubMed: 15783351
- Courtiol, J., Perdikis, D., Petkoski, S., Müller, V., Huys, R., Sleimen-Malkoun, R., et al. (2016). The multiscale entropy: Guidelines for use and interpretation in brain signal analysis. *Journal of Neuroscience Methods*, *273*, 175–190. https://doi.org/10.1016/j.jneumeth.2016.09.004, PubMed: 27639660
- de Boer-Schellekens, L., Eussen, M., & Vroomen, J. (2013).
 Diminished sensitivity of audiovisual temporal order in autism spectrum disorder. *Frontiers in Integrative Neuroscience*, 7, 1–8. https://doi.org/10.3389/fnint.2013.00008, PubMed: 23450453
- Desikan, R. S., Ségonne, F., Fischl, B., Quinn, B. T., Dickerson, B. C., Blacker, D., et al. (2006). An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest. *Neuroimage*, *31*, 968–980. https://doi.org/10.1016/j.neuroimage.2006.01.021, PubMed: 16530430
- Diederich, A., & Colonius, H. (2004). Bimodal and trimodal multisensory enhancement: Effects of stimulus onset and intensity on reaction time. *Perception & Psychophysics*, 66, 1388–1404. https://doi.org/10.3758/BF03195006, PubMed: 15813202
- Driver, J., & Noesselt, T. (2008). Multisensory interplay reveals crossmodal influences on "sensory-specific" brain regions,

neural responses, and judgments. *Neuron*, *57*, 11–23. https://doi.org/10.1016/j.neuron.2007.12.013, PubMed: 18184561

Duncan, N. W., & Northoff, G. (2013). Overview of potential procedural and participant-related confounds for neuroimaging of the resting state. *Journal of Psychiatry* and Neuroscience, 38, 84–96. https://doi.org/10.1503/jpn .120059, PubMed: 22964258

Efron, B., & Tibshirani, R. (1986). Bootstrap methods for standard errors, confidence intervals and other measures of statistical accuracy. *Statistical Science*, *1*, 54–77. https://doi .org/10.1214/ss/1177013815

Engel, A., Fries, P., & Singer, W. (2001). Dynamic predictions: Oscillations and synchrony in top–down processing. *Nature Reviews Neuroscience*, 2, 704–716. https://doi.org/10.1038 /35094565, PubMed: 11584308

Ferri, F., Nikolova, Y. S., Perrucci, M. G., Costantini, M., Ferretti, A., Gatta, V., et al. (2017). A neural "tuning curve" for multisensory experience and cognitive-perceptual schizotypy. *Schizophrenia Bulletin*, 43, 801–813. https://doi .org/10.1093/schbul/sbw174, PubMed: 28168302

Finn, E. S., Scheinost, D., Finn, D. M., Shen, X., Papademetris, X., & Constable, R. T. (2017). Can brain state be manipulated to emphasize individual differences in functional connectivity? *Neuroimage*, *160*, 140–151. https:// doi.org/10.1016/j.neuroimage.2017.03.064, PubMed: 28373122

Fonov, V. S., Evans, A. C., Mckinstry, R. C., Almli, C. R., & Collins, D. L. (2009). Unbiased nonlinear average age-appropriate brain templates from birth to adulthood. *Neuroimage*, 47, S102. https://doi.org/10.1016/S1053-8119(09)70884-5

Foucher, J. R., Lacambre, M., Pham, B. T., Giersch, A., & Elliott, M. A. (2007). Low time resolution in schizophrenia. Lengthened windows of simultaneity for visual, auditory and bimodal stimuli. *Schizophrenia Research*, 97, 118–127. https://doi.org/10.1016/j.schres.2007.08.013, PubMed: 17884350

Fries, P. (2009). Neuronal gamma-band synchronization as a fundamental process in cortical computation. *Annual Review* of *Neuroscience*, 32, 209–224. https://doi.org/10.1146 /annurev.neuro.051508.135603, PubMed: 19400723

Ghazanfar, A. A., & Schroeder, C. E. (2006). Is neocortex essentially multisensory? *Trends in Cognitive Sciences*, 10, 278–285. https://doi.org/10.1016/j.tics.2006.04.008, PubMed: 16713325

Gramfort, A., Papadopoulo, T., Olivi, E., & Clerc, M. (2010). OpenMEEG: Opensource software for quasistatic bioelectromagnetics. *Biomedical Engineering Online*, 9, 45. https://doi.org/10.1186/1475-925X-9-45, PubMed: 20819204

Hahn, N., Foxe, J. J., & Molholm, S. (2014). Impairments of multisensory integration and cross-sensory learning as pathways to dyslexia. *Neuroscience and Biobehavioral Reviews*, 47, 384–392. https://doi.org/10.1016/j.neubiorev .2014.09.007, PubMed: 25265514

Hairston, W. D., Burdette, J. H., Flowers, D. L., Wood, F. B., & Wallace, M. T. (2005). Altered temporal profile of visual-auditory multisensory interactions in dyslexia. *Experimental Brain Research*, *166*, 474–480. https://doi.org/10.1007/s00221-005-2387-6, PubMed: 16028030

Hein, G., & Knight, R. T. (2008). Superior temporal sulcus—It's my area: Or is it? *Journal of Cognitive Neuroscience*, 20, 2125–2136. https://doi.org/10.1162/jocn.2008.20148, PubMed: 18457502

Hershenson, M. (1962). Reaction time as a measure of intersensory facilitation. *Journal of Experimental Psychology*, 63, 289–293. https://doi.org/10.1037/h0039516, PubMed: 13906889 Hillock-Dunn, A., & Wallace, M. T. (2012). Developmental changes in the multisensory temporal binding window persist into adolescence. *Developmental Science*, 15, 688–696. https://doi.org/10.1111/j.1467-7687.2012.01171.x, PubMed: 22925516

Jones, E. G., & Powell, T. P. S. (1970). An anatomical study of converging sensory pathways within the cerebral cortex of the monkey. *Brain*, 93, 793–820. https://doi.org/10.1093 /brain/93.4.793, PubMed: 4992433

Kaganovich, N., & Schumaker, J. (2016). Electrophysiological correlates of individual differences in perception of audiovisual temporal asynchrony. *Neuropsychologia*, 86, 119–130. https://doi.org/10.1016/j.neuropsychologia.2016.04 .015, PubMed: 27094850

Kambe, J., Kakimoto, Y., & Araki, O. (2015). Phase reset affects auditory–visual simultaneity judgment. *Cognitive Neurodynamics*, 9, 487–493. https://doi.org/10.1007/s11571 -015-9342-4, PubMed: 26379799

Keil, J., & Senkowski, D. (2018). Neural oscillations orchestrate multisensory processing. *Neuroscientist*, 24, 1–18. https://doi.org/10.1177/1073858418755352, PubMed: 29424265

Kumar, V. G., Dutta, S., Talwar, S., Roy, D., & Banerjee, A. (2020). Biophysical mechanisms governing large-scale brain network dynamics underlying individual-specific variability of perception. *European Journal of Neuroscience*, 52, 3746–3762. https://doi.org/10.1111/ejn.14747, PubMed: 32304122

Kwakye, L. D., Foss-Feig, J. H., Cascio, C. J., Stone, W. L., & Wallace, M. T. (2011). Altered auditory and multisensory temporal processing in autism spectrum disorders. *Frontiers in Integrative Neuroscience*, *4*, 1–11. https://doi.org/10.3389 /fnint.2010.00129, PubMed: 21258617

Magnotti, J. F., Ma, W. J., & Beauchamp, M. S. (2013). Causal inference of asynchronous audiovisual speech. *Frontiers in Psychology*, 4, 798. https://doi.org/10.3389/fpsyg .2013.00798, PubMed: 24294207

Makeig, S., Bell, A. J., Jung, T.-P., & Sejnowski, T. J. (1996).
Independent component analysis of electroencephalographic data. In D. S. Touretzky, M. C. Mozer, & M. E. Hasselmo (Eds.), *Advances in neural information processing systems* (Vol. 8, pp. 145–151). Cambridge, MA: MIT Press.

- Marchant, J. L., Ruff, C. C., & Driver, J. (2012). Audiovisual synchrony enhances BOLD responses in a brain network including multisensory STS while also enhancing target-detection performance for both modalities. *Human Brain Mapping*, *33*, 1212–1224. https://doi.org/10.1002/hbm .21278, PubMed: 21953980
- Martin, B., Giersch, A., Huron, C., & van Wassenhove, V. (2013).
 Temporal event structure and timing in schizophrenia: Preserved binding in a longer "now." *Neuropsychologia*, *51*, 358–371. https://doi.org/10.1016/j.neuropsychologia.2012.07
 .002, PubMed: 22813430

McIntosh, A. R., Bookstein, F. L., Haxby, J. V., & Grady, C. L. (1996). Spatial pattern analysis of functional brain images using partial least squares. *Neuroimage*, 157, 143–157. https://doi.org/10.1006/nimg.1996.0016, PubMed: 9345485

McIntosh, A. R., Kovacevic, N., & Itier, R. J. (2008). Increased brain signal variability accompanies lower behavioral variability in development. *PLoS Computational Biology*, *4*, e1000106. https://doi.org/10.1371/journal.pcbi.1000106, PubMed: 18604265

McIntosh, A. R., & Lobaugh, N. J. (2004). Partial least squares analysis of neuroimaging data: Applications and advances. *Neuroimage*, 23, 250–263. https://doi.org/10.1016/j .neuroimage.2004.07.020, PubMed: 15501095

Miller, L. M., & D'Esposito, M. (2005). Perceptual fusion and stimulus coincidence in the cross-modal integration of speech. *Journal of Neuroscience*, 25, 5884–5893. https://doi.org/10.1523/JNEUROSCI.0896-05.2005, PubMed: 15976077

Monosov, I. E., Haber, S. N., Leuthardt, E. C., & Jezzini, A. (2020). Anterior cingulate cortex and the control of dynamic behavior in primates. *Current Biology*, *30*, R1442–R1454. https://doi.org/10.1016/j.cub.2020.10.009, PubMed: 33290716

Morcom, A. M., & Fletcher, P. C. (2007). Does the brain have a baseline? Why we should be resisting a rest. *Neuroimage*, *37*, 1073–1082. https://doi.org/10.1016/j.neuroimage.2006.09 .013, PubMed: 17681817

Murray, M. M., Eardley, A. F., Edginton, T., Oyekan, R., Smyth, E., & Matusz, P. J. (2018). Sensory dominance and multisensory integration as screening tools in aging. *Scientific Reports*, *8*, 8901. https://doi.org/10.1038/s41598-018 -27288-2, PubMed: 29891964

Nath, A. R., & Beauchamp, M. S. (2012). A neural basis for interindividual differences in the McGurk effect, a multisensory speech illusion. *Neuroimage*, 59, 781–787. https://doi.org/10.1016/j.neuroimage.2011.07.024, PubMed: 21787869

Noesselt, T., Rieger, J. W., Schoenfeld, M. A., Kanowski, M., Hinrichs, H., Heinze, H.-J., et al. (2007). Audiovisual temporal correspondence modulates human multisensory superior temporal sulcus plus primary sensory cortices. *Journal of Neuroscience*, *27*, 11431–11441. https://doi.org/10.1109/SENSOR.2007.4300668, PubMed: 17942738

Pascual-Marqui, R. D. (2002). Standardized low resolution brain electromagnetic tomography (sLORETA): Technical details. *Methods and Findings in Experimental and Clinical Pharmacology, 24 Suppl. D*, 5–12.

Peirce, J., Gray, J. R., Simpson, S., Macaskill, M., Höchenberger, R., Sogo, H., et al. (2019). PsychoPy2: Experiments in behavior made easy. *Behavior Research Methods*, *51*, 195–203. https://doi.org/10.3758/s13428-018-01193-y, PubMed: 30734206

Powers, A. R., Hevey, M. A., & Wallace, M. T. (2012). Neural correlates of multisensory perceptual learning. *Journal of Neuroscience*, *32*, 6263–6274. https://doi.org/10.1523 /jneurosci.6138-11.2012, PubMed: 22553032

Powers, A. R., Hillock, A. R., & Wallace, M. T. (2009). Perceptual training narrows the temporal window of multisensory binding. *Journal of Neuroscience*, 29, 12265–12274. https:// doi.org/10.1523/JNEUROSCI.3501-09.2009, PubMed: 19793985

Sampson, P. D., Streissguth, P., Barr, H. M., & Bookstein, F. L. (1989). Neurobehavioural effects of prenatal alcohol. Part II. Partial least squares analysis. *Neurotoxicology and Teratology*, *11*, 477–491. https://doi.org/10.1016/0892-0362 (89)90025-1, PubMed: 2593987

Schroeder, C. E., & Foxe, J. J. (2002). The timing and laminar profile of converging inputs to multisensory areas of the macaque neocortex. *Cognitive Brain Research*, 14, 187–198. https://doi.org/10.1016/s0926-6410(02)00073-3, PubMed: 12063142

Senkowski, D., Schneider, T. R., Foxe, J. J., & Engel, A. K. (2008). Crossmodal binding through neural coherence: Implications for multisensory processing. *Trends in Neurosciences*, *31*, 401–409. https://doi.org/10.1016/j.tins .2008.05.002, PubMed: 18602171

Shams, L., & Seitz, A. R. (2008). Benefits of multisensory learning. *Trends in Cognitive Sciences*, 30, 1–7. https://doi .org/10.1016/j.tics.2008.07.006, PubMed: 18805039

Spitmaan, M., Seo, H., Lee, D., & Soltani, A. (2020). Multiple timescales of neural dynamics and integration of task-relevant signals across cortex. *Proceedings of the National Academy* of Sciences, U.S.A., 117, 22522–22531. https://doi.org/10.1073 /pnas.2005993117, PubMed: 32839338

Stevenson, R. A., Altieri, N. A., Kim, S., Pisoni, D. B., & James, T. W. (2010). Neural processing of asynchronous audiovisual speech perception. *Neuroimage*, 49, 3308–3318. https://doi.org/10.1016/j.neuroimage.2009.12.001, PubMed: 20004723

Stevenson, R. A., VanDerKlok, R. M., Pisoni, D. B., & James, T. W. (2011). Discrete neural substrates underlie complementary audiovisual speech integration processes. *Neuroimage*, 55, 1339–1345. https://doi.org/10.1016/j.neuroimage.2010.12 .063, PubMed: 21195198

Stevenson, R. A., & Wallace, M. T. (2013). Multisensory temporal integration: Task and stimulus dependencies. *Experimental Brain Research*, 227, 249–261. https://doi.org/10.1007/s00221 -013-3507-3, PubMed: 23604624

Stevenson, R. A., Wilson, M. M., Powers, A. R., & Wallace, M. T. (2013). The effects of visual training on multisensory temporal processing. *Experimental Brain Research*, 225, 479–489. https://doi.org/10.1007/s00221-012-3387-y, PubMed: 23307155

Stevenson, R. A., Zemtsov, R. K., & Wallace, M. T. (2012). Individual differences in the multisensory temporal binding window predict susceptibility to audiovisual illusions. *Journal of Experimental Psychology: Human Perception and Performance*, *38*, 1517–1529. https://doi.org/10.1037 /a0027339, PubMed: 22390292

Sumby, W. H., & Pollack, I. (1954). Visual contribution to speech intelligibility in noise. *Journal of the Acoustical Society of America*, 26, 212–215. https://doi.org/10.1121/1 .1907309

- Tadel, F., Baillet, S., Mosher, J. C., Pantazis, D., & Leahy, R. M. (2011). Brainstorm: A user-friendly application for MEG/EEG analysis. *Computational Intelligence and Neuroscience*, 2011, 1–13. https://doi.org/10.1155/2011/879716, PubMed: 21584256
- Vakorin, V. A., Lippé, S., & McIntosh, A. R. (2011). Variability of brain signals processed locally transforms into higher connectivity with brain development. *Journal of Neuroscience*, *31*, 6405–6413. https://doi.org/10.1523/JNEUROSCI.3153-10 .2011, PubMed: 21525281
- van Atteveldt, N., Murray, M. M., Thut, G., & Schroeder, C. E. (2014). Multisensory integration: Flexible use of general operations. *Neuron*, 81, 1240–1253. https://doi.org/10.1016/j .neuron.2014.02.044, PubMed: 24656248
- van Eijk, R. L. J., Kohlrausch, A., Juola, J. F., & van de Par, S. (2008). Audiovisual synchrony and temporal order judgments: Effects of experimental method and stimulus type. *Perception & Psychophysics*, 70, 955–968. https://doi.org/10.3758/PP.70.6.955, PubMed: 18717383
- Wallace, M. T., Woynaroski, T. G., & Stevenson, R. A. (2020). Multisensory integration as a window into orderly and disrupted cognition and communication. *Annual Review of Psychology*, 71, 193–219. https://doi.org/10.1146/annurev -psych-010419-051112, PubMed: 31518523

Yarrow, K., (2018). Collecting and interpreting judgments about perceived simultaneity: A model-fitting tutorial. In A. Vatakis, F. Balcı, M. Di Luca, & Á. Correa (Eds.), *Timing and time perception: Procedures, measures, & applications* (pp. 295–325). Leiden, The Netherlands: Brill. https://doi.org/10.1163 /9789004280205 014

Yarrow, K., (2020). MATLAB code to implement fits of psychophysical observer models to data from behavioural timing tasks (SJ, TOJ, 2xSJ, ternary) (Version 1). City, University of London. https://doi.org/10 .25383/city.11848263.v1 Yarrow, K., Jahn, N., Durant, S., & Arnold, D. H. (2011). Shifts of criteria or neural timing? The assumptions underlying timing perception studies. *Consciousness and Cognition*, 20, 1518–1531. https://doi.org/10.1016/j.concog.2011.07.003

Yuan, X., Li, H., Liu, P., Yuan, H., & Huang, X. (2016). Pre-stimulus beta and gamma oscillatory power predicts perceived audiovisual simultaneity. *International Journal of Psychophysiology*, *107*, 29–36. https://doi.org/10.1016/j .ijpsycho.2016.06.017, PubMed: 27393081

- Zhang, Y. (1991). Complexity and 1/f noise. A phase space approach. *Journal de Physique I*, *1*, 971–977. https://doi.org /10.1051/jp1:1991180
- Zmigrod, L., & Zmigrod, S. (2016). On the temporal precision of thought: Individual differences in the multisensory temporal binding window predict performance on verbal and nonverbal problem solving tasks. *Multisensory Research*, 29, 679–701. https://doi.org/10.1163/22134808 -00002532